

A multi-transmitter multi-receiver model for molecular communication networks

Chun Tung Chou

School of Computer Science and Engineering
University of New South Wales, Australia
ctchou@cse.unsw.edu.au

Technical Report
UNSW-CSE-TR-201202
February 2012

THE UNIVERSITY OF
NEW SOUTH WALES



School of Computer Science and Engineering
The University of New South Wales
Sydney 2052, Australia

Abstract

We consider molecular communication networks consisting of transmitters and receivers distributed in a fluidic medium. In such networks, a transmitter sends one or signalling molecules, which are diffused over the medium, to the receiver to realise the communication. In order to be able to engineer synthetic molecular communication networks, a mathematical model for these networks is required. This paper proposes a new stochastic model of molecular communication networks called reaction-diffusion master equation with exogenous input (RDMEX). An advantage of RDMEX is that it can readily be used to model molecular communication networks with multiple transmitters and receivers. For the case where the reaction kinetics at the receivers is linear, we show how RDMEX can be used to determine the mean and covariance behaviour of molecular communication networks, and derive closed-form expressions for the mean behaviour of the RDMEX model. These closed-form expressions offer insight into how the transmitters and receivers interfere with each other. Numerical examples are provided to demonstrate the properties of the model.

1 Introduction

We consider molecular communication networks consisting of transmitters and receivers distributed in a fluidic medium. In such networks, a transmitter sends one or signalling molecules, which are diffused over the medium, to the receiver to realise the communication. The study of molecular communication has its origin in biology and biophysics. Molecular communication is a vital mechanism in a multi-cellular organism. The human body, which has an estimated 10^{14} cells, uses molecular communication to keep the body in a healthy state. In fact, cells in the human body constantly communicate with other cells using molecular communication.

There are a couple of reasons why synthetic molecular communication networks, which are inspired by molecular communication in living organisms, should be studied. Firstly, synthetic molecular communication networks can be combined with nano-sensors and molecular computing [28] to form nano-sensor networks for health monitoring, medical diagnosis and cancer therapy [3, 1]. Secondly, the study of synthetic molecular communication networks can be used to enhance our understanding of their biological counterparts.

In order to be able to engineer synthetic molecular communication networks, we need mathematical models which can be used to predict the performance of these networks. The main contribution of this paper is that we propose a new stochastic model for molecular communication networks. Our model is based on reaction-diffusion master equation (RDME) [14] which is a well known model in physics for modelling systems with both diffusion and chemical reactions. In this paper, we propose an extension to RDME, which we call reaction-diffusion master equation with exogenous input (RDME_X), to model molecular communication networks with many transmitters and many receivers. For the case where the reaction kinetics at the receivers is linear, we show how RDME_X can be used to determine the mean and covariance behaviour of molecular communication networks. These results allow us to derive closed-form expressions showing how the receiver outputs relate to the transmitter signals when there are multiple transmitters and receivers. These expressions also provide us insights with how transmitters and receivers interfere with each others.

This paper is organised as follows. In Section 2, we present background materials on master equations which are stochastic models commonly used to model chemical reactions and diffusion. In Section 3, we present the RDME_X and show how it can be used to model molecular communication networks with multiple transmitters and receivers. We also show in this section how we can determine the mean and covariance of the receiver behaviour in molecular communication networks. The rest of the paper is focused on determining the mean receiver behaviour. We approach this by using two methods, which will be discussed in sections 4 and 5. In Section 4, we determine the continuum limit of the RDME_X and show that it results in a reaction-diffusion partial differential equation (RDPDE). We derive a closed-form solution of this RDPDE. The solution provides us insights on how different transmitter-receiver pairs in a molecular communication network interfere with each other. In Section 5, we determine the mean receiver behaviour of RDME_X with finite spatial resolution and derive another closed-form solution. Numerical results are then presented in section 6 to illustrate some properties of molecular communication networks. Finally, section 7 describes the related work and section 8 gives the conclusions.

2 Background on master equations

The aim of this section is to provide the necessary background on master equations. The treatment here is brief and includes only the results needed for this article. The reader can refer to the texts [14, 27] or tutorial article [12] for a more complete treatment of the subject. This section is divided into two parts. We first introduce the general master equation and give a simple example on how to use master equation to model a chemical reaction. We then quote some results on mean and covariance of the Markov processes modelled by a master equation.

2.1 General master equation

Consider a continuous-time integer-value vector Markov process $Q(t) \in \mathbb{Z}^p$, where p is the number of vector components, \mathbb{Z} is the set of all integers and t is time. When the Markov process $Q(t)$ is in state $q \in \mathbb{Z}^p$, it jumps to the state $q + r_j$ (where $r_j \in \mathbb{Z}^p$ with $j = 1, 2, \dots, J$ and J is the total number of possible jumps) at a transition rate of $W_j(q)$. Let $P(q, t|q_0, t_0)$ denote the conditional probability that $Q(t) = q$ given that $Q(t_0) = q_0$.

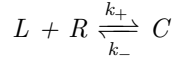
We are interested to determine how $P(q, t|q_0, t_0)$ evolves over time. We can do this by using a coupled set of ODEs known as the master equation:

$$\frac{dP(q, t|q_0, t_0)}{dt} = \sum_{j=1}^J W_j(q - r_j)P(q - r_j, t|q_0, t_0) - \sum_{j=1}^J W_j(q)P(q, t|q_0, t_0) \quad (2.1)$$

where one equation of the form (2.1) is needed for each valid state q . Note that the first and second terms on the right-hand side of (2.1) can be interpreted, respectively, as the rates of entering and leaving the state q . In order to simplify notation, we will write $P(q, t)$ instead of $P(q, t|q_0, t_0)$ from now on.

A common application of master equation is to model the dynamics of chemical reactions. We will give a simple example to illustrate that.

Example 1 Consider the chemical reaction:



where the chemical species are L , R and C , and the forward and reverse reaction constants are k_+ and k_- respectively. This chemical reaction can be described by a Markov process with state space $q = [n_L, n_R, n_C]^T$ where n_L is the number of molecules of chemical L etc., and T denotes matrix transpose.

There are two possible types of jumps (i.e. $J = 2$) in this system. The forward reaction is modelled by the jump $r_1 = [-1, -1, 1]^T$ where the entries of r_1 reflects the fact that one molecule of L and one molecule of R react to form a molecule of C . The rate of jump, which according to standard result in chemical kinetics, is $W_1(q) = k_+q(1)q(2) = k_+n_Ln_R$ where $q(1)$ is the first component of the vector q , etc. Similarly, the reverse reaction is modelled by the jump $r_2 = [1, 1, -1]^T$ with $W_2(q) = k_-q(3) = k_-n_C$. The master equation for this chemical reaction is:

$$\frac{dP(q, t)}{dt} = \sum_{j=1}^2 W_j(q - r_j)P(q - r_j, t) - \sum_{j=1}^2 W_j(q)P(q, t) \quad (2.2)$$

Equations of the type (2.2) is also known as chemical master equations.

2.2 Results on mean and covariance

The master equation (2.1) shows the time evolution of the state probability of the Markov process $Q(t)$. However, (2.1) can be difficult to work with because we need one equation for each valid state, hence the number of equations can be very large. Therefore, it is easier if we can determine the mean and covariance of the Markov process $Q(t)$, which is defined as follows:

$$\langle Q(t) \rangle = \sum_q q \text{Prob}(Q(t) = q) = \sum_q qP(q, t) \quad (2.3)$$

$$\Sigma(t) = \sum_q (q - \langle Q(t) \rangle)(q - \langle Q(t) \rangle)^T P(q, t) \quad (2.4)$$

where $\langle \bullet \rangle$ will be used in this paper to denote the mean operator.

It is possible to use (2.1) to derive how the mean and covariance of the state of the Markov process $Q(t)$ evolve over time. The following proposition is taken from [20].

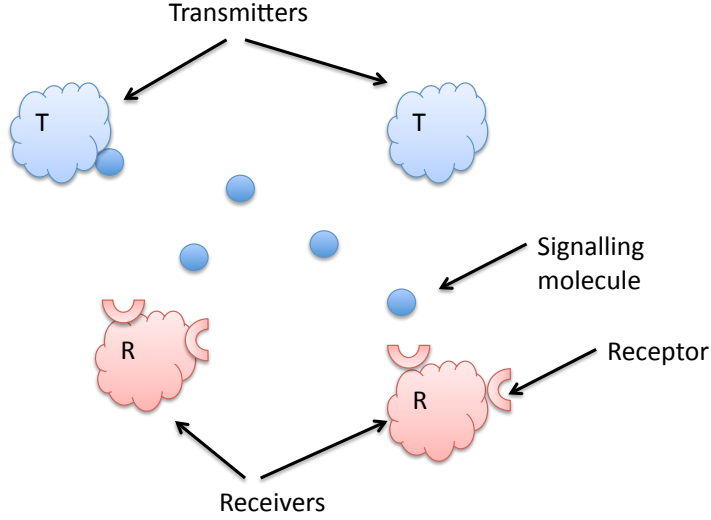


Figure 3.1: An illustration of a molecular communication network with two transmitters and two receivers. The signalling molecules diffuse in a fluidic medium and may bind with the receptors at the receivers.

Proposition 1 *For the general master equation (2.1), we have*

$$\frac{d\langle Q(t) \rangle}{dt} = \sum_{j=1}^J r_j \langle W_j(Q(t)) \rangle \quad (2.5)$$

In particular, if $W_j(q)$ is a linear function of q . Let $\sum_{j=1}^J r_j W_j(q) = Aq$, then

$$\frac{d\langle Q(t) \rangle}{dt} = A\langle Q(t) \rangle \quad (2.6)$$

$$\frac{d\Sigma(t)}{dt} = A\Sigma(t) + \Sigma(t)A^T + \sum_{j=1}^J r_j r_j^T W_j(\langle Q(t) \rangle) \quad (2.7)$$

3 Modelling molecular communication network using RD-MEX

We consider a molecular communication network with multiple transmitters and multiple receivers in an isotropic fluidic medium, see Figure 3.1. The communication takes place by the transmitter emitting one or more signalling molecules over time. Once the molecules leave the transmitter, they diffuse in the medium according to Brownian motion. The receivers are assumed to consist of one or more receptors. When a signalling molecule L reaches a receptor R , they may bind together to form a complex C . We will consider the number of complexes at the receiver as the output of the receiver. For example, a receiver may infer that a bit has been sent by the transmitter when the number of complexes exceeds a threshold.

Based on the above description, we see that a model for molecular communication networks must at least capture the diffusion of signalling molecules and the reactions at the receivers. Both reactions and diffusion can be modelled as Markov processes, so the master equation (2.1) is a natural choice. The remaining issue is how we can model the transmitter. In this paper, we model the transmitter by a time sequence which specifies the number of molecules emitted by

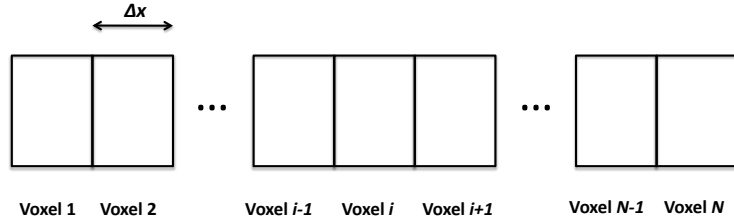


Figure 3.2: The voxels in the 1-dimensional RDMEX model.

the transmitter at a particular time. This approach is fairly general and can be used to model encoding methods that have been considered in the literature, such as molecular coding [1] and concentration coding [22]. We will consider other modelling approaches, e.g. modelling the internal mechanism of the transmitters, in future work.

In section 3.1, we will introduce the RDMEX model by way of an example and then we will prove some results on mean and covariance of the RDMEX model in section 3.2.

3.1 The RDMEX model

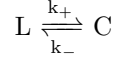
In this section, we will introduce the RDMEX model for a molecular communication network with 2 transmitters, 2 receivers in a 1-dimensional medium. The reason for that is to simplify the presentation. It is fairly simple to generalise the model to multiple transmitters, multiple receivers in a 3-dimensional medium, which we will discuss at the end of the section.

Another simplification is that we will assume, at the receiver, the rate at which the complexes are formed is a linear function of the number of local signalling molecules and is independent of the number of receptors. (This will be made precise below.) This simplification allows us to produce closed form expressions in the continuum limit which provide us with insight into the interference structure of the network. Note that, it is straightforward to model non-linear reaction rates or incorporate more complex receivers in our model.

The following is a list of model assumptions, parameters and notation.

1. We assume that both transmitters use one and the same type of signalling molecule L .
2. For transmitter 1, we assume that it emits $k_{1,1}$ signalling molecules of L at time $t_{1,1}$, $k_{1,2}$ molecules of L at time $t_{1,2}$, ..., $k_{1,b}$ molecules of L at time $t_{1,b}$, where $k_{1,b}$ ($b = 1, 2, 3, \dots$) are positive integers and $t_{1,b} \in \mathbb{R}$. Similarly, transmitter 2 emits $k_{2,b}$ signalling molecules of L at $t_{2,b}$ where $b = 1, 2, 3, \dots$. The number of molecules emitted $k_{a,b}$ is assumed to be independent of the state of the system.
3. The medium is assumed to be a 1-dimensional space of length X . The medium is partitioned into N equal width voxels of width Δx such that $N \Delta x = X$. We index the voxels by using $1, \dots, N$. See Figure 3.2 for an illustration.
4. The medium is assumed to be isotropic. The rate at which a signalling molecule L diffuses from one voxel to a neighbouring voxel is d per molecule per unit time. The rate of diffusion from a voxel to a non-neighbouring voxel is zero. Also, the molecule cannot leave the medium and we assume the boundary is reflective.
5. We assume that each transmitter or receiver occupies only one voxel. Transmitters 1 and 2 are located respectively in the voxel indexed by T_1 and T_2 . Similarly, we assume that receivers 1 and 2 are located in the voxels indexed by R_1 and R_2 . The indices T_1 , T_2 , R_1 and R_2 are integers in the interval $[1, N]$ and are assumed to be distinct. (Note that it is simple to modify the model so that a transmitter or a receiver occupies multiple voxels.)

6. We assume both receivers 1 and 2 use the same type of receptors R and these receptors are fixed in space, i.e. do not diffuse. With the simplification mentioned in the introductory part of this section, we assume that the reaction between the signalling molecule L and the complex C is:



With this assumption, the rate of formation of complexes at receiver 1, at any time, is proportional to the number of signalling molecules L in the R_1 -th voxel. The situation at receiver 2 is similar.

7. The state vector q consists of $(N + 2)$ elements where

$$q = [n_{L,1} \quad n_{L,2} \quad \dots \quad n_{L,N} \quad n_{C,1} \quad n_{C,2}] \quad (3.1)$$

where $n_{L,j}$ represents the number of signalling molecules at the j -th voxel and $n_{C,u}$ represents the number of complexes at the u -th receiver.

8. We define two indicator vectors $\mathbb{1}_{T_1}, \mathbb{1}_{T_2} \in \mathbb{Z}^{N+2}$. The T_1 -th element of $\mathbb{1}_{T_1} = \mathbb{1}_{T_1}(T_1) = 1$ and are otherwise zero. $\mathbb{1}_{T_2}$ is similarly defined.
9. In order to write down the diffusion and reaction within the molecular communication network, we define the following state transition vectors r_j and transition rates W_j . The total number of possible jumps in this system is $J = 2N + 4$ where $2N$ of them model diffusion and the rest models reactions at the receivers. We will state these jumps below in four categories. Note that all $r_j \in \mathbb{Z}^{N+2}$ and only the non-zero elements are stated, and q is the state vector defined in (3.1).

- (a) The diffusion of L from voxel j to $j + 1$, where $1 \leq j \leq N - 1$, is modelled by r_j and $W_j(q)$. Specifically, $r_j(j) = -1$, $r_j(j + 1) = 1$ and $W_j(q) = \mathfrak{d}q(j) = \mathfrak{d}n_{L,j}$.

Explanation: If a signalling molecule diffuses from voxel j to $j + 1$, it means the number of molecules in voxel j is decreased by one (hence $r_j(j) = -1$) and that in voxel $j + 1$ is increased by one (hence $r_j(j + 1) = 1$). The rate at which this particular jump takes place is proportional to the number of molecules in the j -th voxel, which is given by the j -th element of the state vector q .

For convenience, we define r_N to be a zero vector and $W_N(q) = 0$.

- (b) For the diffusion of L from voxel j to $j - 1$ where $2 \leq j \leq N$, $r_{N+j}(j) = -1$, $r_{N+j}(j - 1) = 1$ and $W_{N+j}(q) = \mathfrak{d}q(j) = \mathfrak{d}n_{L,j}$. For convenience, we define r_{N+1} to be a zero vector and $W_{N+1}(q) = 0$.

- (c) For receiver 1, the vector r_{2N+1} and the rate $W_{2N+1}(q)$ are used to model the forward reaction of the conversion of a signalling molecule L to a complex C . Specifically, $r_{2N+1}(R_1) = -1$, $r_{2N+1}(N + 1) = 1$ and $W_{2N+1}(q) = k_+q(R_1) = k_+n_{L,R_1}$.

Explanation: In the forward reaction, a signalling molecule is removed in the R_1 -th voxel, hence $r_{2N+1}(R_1) = -1$ and a complex is formed, hence $r_{2N+1}(N + 1) = 1$ because the number of complexes at receiver 1 is the $(N + 1)$ -th element in the state vector (3.1). The rate $W_{2N+1}(q)$ is proportional to the number of signalling molecules in the R_1 -th voxel where the receiver is located.

For the reverse reaction, $r_{2N+2}(N + 1) = -1$, $r_{2N+2}(R_1) = 1$ and $W_{2N+2}(q) = k_-q(N + 1) = k_-n_{C,1}$.

- (d) For receiver 2, the forward reaction: $r_{2N+3}(R_2) = -1$, $r_{2N+3}(N + 2) = 1$ and $W_{2N+3}(q) = k_+q(R_2) = k_+n_{L,R_2}$. For the reverse reaction, $r_{2N+4}(N + 2) = -1$, $r_{2N+4}(R_2) = 1$ and $W_{2N+4}(q) = k_-q(N + 2) = k_-n_{C,2}$.

The RDMEX model for the 2-transmitter 2-receiver molecular communication network is

$$\begin{aligned} \frac{dP(q, t)}{dt} = & \sum_{a=1}^2 \sum_{b=1}^{\infty} \{P(q - k_{a,b} \mathbb{1}_{T_a}) - P(q, t)\} \delta(t - t_{a,b}) \\ & + \sum_{j=1}^J W_j(q - r_j) P(q - r_j, t) - \sum_{j=1}^J W_j(q) P(q, t) \end{aligned} \quad (3.2)$$

where $\delta(t)$ denotes the Dirac delta function.

Let us, for the time being, assume that the first term on the right-hand side of (3.2) is not there. If this is the case, then (3.2) is of the same form as the master equation (2.1) and the equation models a Markov process. Given this model includes both reaction and diffusion, equation (3.2) without the first term is known in the literature as reaction-diffusion master equation (RDME).

The novelty of the RDMEX model is the introduction of the first term on the right-hand side of (3.2). This term can be viewed as a deterministic input because molecules are emitted by the transmitters at pre-determined times. Let us look at this term more closely. At time $t_{a,b}$, the a -th transmitter emits $k_{a,b}$ signalling molecules into the T_a -th voxel (where the a -th transmitter is located). This means that if the system is in the state q just before the time $t_{a,b}$ (denoted as $t_{a,b}^-$), then it will be in state $q + k_{a,b} \mathbb{1}_{T_a}$ just after $t_{a,b}$ (denoted as $t_{a,b}^+$). In addition, we have $P(q, t_{a,b}^-) = P(q + k_{a,b} \mathbb{1}_{T_a}, t_{a,b}^+)$, which is the mathematical meaning of the first term in (3.2). Note that it is possible to give a stochastic interpretation of $k_{a,b}$, see the last paragraph in section 3.2.

The deterministic input in (3.2) can be thought of an external arrival of the system. We will refer to (3.2) as reaction-diffusion master equation with exogenous input, or RDMEX for short. The name is inspired by time series models such as ARX and ARMAX [21].

Note that the RDMEX model is no longer a Markov process due to the deterministic arrivals. However, RDMEX is piecewise Markovian in the sense that, it is Markovian in between two consecutive deterministic arrivals.

We have given an example of RDMEX for a 2-transmitter 2-receiver model in 1-dimension. The model can be readily generalised to include more transmitters and receivers. In order to generalise the model to 3-dimensional space, we will need to divide the space into 3-dimensional cubic voxels of equal volume. (The use of more complicated geometry is possible, see [18].) The molecules in a voxel are only allowed to diffuse to any of its neighbouring voxels. This can also be readily be done. Lastly, we remark that it is also possible to use more complex receiver structure or to consider non-isotropic medium.

3.2 Mean and covariance of RDMEX

We will now generalise the result of Proposition 1 to the case of RDMEX model.

Proposition 2 *For the RDMEX model in (3.2), assuming that $W_j(q)$ is a linear function of q . Let $\sum_{j=1}^J r_j W_j(q) = Aq$, then*

$$\frac{d\langle Q(t) \rangle}{dt} = A\langle Q(t) \rangle + \sum_{a=1}^2 \sum_{b=1}^{\infty} k_{a,b} \mathbb{1}_{T_a} \delta(t - t_{a,b}) \quad (3.3)$$

$$\frac{d\Sigma(t)}{dt} = A\Sigma(t) + \Sigma(t)A^T + \sum_{j=1}^J r_j r_j^T W_j(\langle x(t) \rangle) \quad (3.4)$$

Proof: For the time evolution on the mean $\langle Q(t) \rangle$, we can start with the derivative of (2.3): $\frac{d\langle Q(t) \rangle}{dt} = \sum_q q \frac{dP(q, t)}{dt}$ and then use (3.2) for $\frac{dP(q, t)}{dt}$. This is fairly straightforward and uses exactly the same argument as the proof in [20].

Alternatively, one can argue the correctness of (3.3) as follows. Given that the difference between (2.1) and (3.2) is the deterministic arrivals modelled by impulses, this means that between

two consecutive deterministic arrivals, the evolution of the state in RDMEX can be described by a standard master equation. Hence, (2.6) holds between two consecutive deterministic arrivals. It can be readily shown that the effect of $k_{a,b}$ molecules arriving at time $t_{a,b}$ is to add $k_{a,b}\mathbb{1}_{T_a}$ to the state vector. Hence the form of (3.3).

For the evolution of covariance, one can follow the derivation in [20] provided that the impulses are handled correctly because the multiplication of Dirac deltas (or distributions) is not well defined. However, one can argue the correctness of (3.4) using the same argument in the last paragraph. We know that between two consecutive deterministic arrivals, (2.7) holds for the RDMEX model. It remains to show that there is no jump in covariance matrix before and after a deterministic arrival.

Let $Q(t_{a,b}^-)$ and $\langle Q(t_{a,b}^-) \rangle$ be the state and mean state just before the deterministic arrival at time $t_{a,b}$. At time $t_{a,b}^+$, just after $t_{a,b}$, the state of the system will become $Q(t_{a,b}^-) + k_{a,b}\mathbb{1}_{T_a}$. Also, the mean state at $t_{a,b}^+$ is:

$$\begin{aligned} \langle Q(t_{a,b}^+) \rangle &= \sum_q q P(q, t_{a,b}^+) = \sum_q q P(q - k_{a,b}\mathbb{1}_{T_a}, t_{a,b}^-) \\ &= \sum_q (q + k_{a,b}\mathbb{1}_{T_a}) P(q, t_{a,b}^-) = \langle Q(t_{a,b}^-) \rangle + k_{a,b}\mathbb{1}_{T_a} \end{aligned}$$

Note that we have used the fact that $P(q, t_{a,b}^+) = P(q - k_{a,b}\mathbb{1}_{T_a}, t_{a,b}^-)$ in the above derivation. The overall result is that, at time $t_{a,b}$, the state $Q(t)$ and mean state $\langle Q(t) \rangle$ are incremented by the same vector $k_{a,b}\mathbb{1}_{T_a}$.

Given that, at any deterministic arrival, both the state and mean state change by exactly the same amount, therefore, deterministic arrivals do not cause discontinuity in covariance. Hence (3.4). \square

For the rest of the paper, we will focus on studying the properties of equation (3.3). A detail study on (3.4) is also important and will be done in a future paper.

We will now briefly discuss a generalisation of the RDMEX model. Instead of assuming a deterministic emission of exactly $k_{a,b}$ signalling molecules by the a -th transmitter at time $t_{a,b}$, one may assume that the number of molecules emitted is a random variable $K_{a,b}$ with mean $\langle K_{a,b} \rangle$ and covariance $\text{cov}(K_{a,b})$. Provided that the random variable $K_{a,b}$ is independent of the state q , similar results to Proposition 2 can be derived. For equation (3.3), we need to replace $k_{a,b}$ by $\langle K_{a,b} \rangle$, and we need to add $\text{cov}(K_{a,b})$ to the right-hand side of (3.4). This generalisation says that one can interpret $k_{a,b}$ in (3.3) as the mean number of molecules emitted at time $t_{a,b}$ by the a -th transmitter.

4 Continuum limit of RDMEX

In section 3.1, we presented an example of the RDMEX model for a 2-transmitter, 2-receiver molecular communication network in an isotropic 1-dimensional medium. We also show that if the reaction dynamics at the receiver is linear, then the mean number of molecules in the network evolves according to the ordinary differential equation (ODE) (3.3). In section 4.1, we will determine the continuum limit of (3.3) as $\Delta x \rightarrow 0$. In order to simplify the presentation, we have so far limited our study to 1-dimensional but given most molecular communication networks are 3-dimensional, we will generalise the continuum limit to 3-dimensional case as well.

The continuum limit of the RDMEX is in fact a RDPDE. A nice property of the resulting RDPDE is that a closed form solution is available. This closed form solution shows explicitly how the transmitters and receivers interfere with each other in a molecular communication network. This will be discussed in section 4.2.

4.1 Continuum limit and generalisation to 3-dimensional space

In this section, we will study the continuum limit of equation (3.3) and show that in the limit, when the interval Δx goes to zero, (3.3) converges to a RDPDE and a number of chemical kinetics ODEs. In order that we will be able to solve the RDPDE analytically later on, we will assume from now onwards that the 1-dimensional medium is infinite, which means that the molecules in each voxel can diffuse to either of its neighbouring voxel and the state vector q is

$$q = [\dots \ n_{L,-1} \ n_{L,0} \ n_{L,1} \ n_{L,2} \ \dots \ n_{L,N} \ n_{C,1} \ n_{C,2}] \quad (4.1)$$

where, as before, $n_{L,j}$ is the number of L in the j -th voxel where $j \in \mathbb{Z}$, and $n_{C,u}$ is the number of complexes formed at the u -th receiver. Given this state vector, we can write equation (3.3) as

$$\begin{aligned} \frac{d\langle n_{L,j}(t) \rangle}{dt} &= \mathfrak{d}(\langle n_{L,j-1}(t) \rangle - 2\langle n_{L,j}(t) \rangle + \langle n_{L,j+1}(t) \rangle) + \sum_{a=1}^2 \sum_{b=1}^{\infty} \delta_K(j - T_a) k_{a,b} \delta(t - t_{a,b}) \\ &\quad - \sum_{u=1}^2 \delta_K(j - R_u) (k_+ \langle n_{L,R_u}(t) \rangle - k_- \langle n_{C,u}(t) \rangle) \quad \forall j \in \mathbb{Z} \end{aligned} \quad (4.2)$$

$$\frac{d\langle n_{C,u}(t) \rangle}{dt} = k_+ \langle n_{L,R_u}(t) \rangle - k_- \langle n_{C,u}(t) \rangle \quad \text{for } u = 1, 2 \quad (4.3)$$

where $\delta_K(j)$ is the Kronecker delta¹.

Suppose the centre of the voxel j is at position x_j , we replace $\langle n_{L,j}(t) \rangle$ by $\ell(x_j, t)\Delta x$ where $\ell(x_j, t)$ is the mean concentration in voxel j at time t . By dividing both sides of (4.2) by Δx , taking the limit $\Delta x \rightarrow 0$ and assuming that $\mathfrak{d}(\Delta x)^2 \rightarrow \check{D}$ and $k_+ \Delta x \rightarrow \check{K}_+$, we have

$$\frac{\partial \ell}{\partial t} = \check{D} \frac{\partial^2 \ell}{\partial x^2} + \sum_{a=1}^2 \delta(x - x_{T,a}) \underbrace{\sum_{b=1}^{\infty} k_{a,b} \delta(t - t_{a,b})}_{=k_a(t)} - \sum_{u=1}^2 \delta(x - x_{R,u}) \frac{d\langle n_{C,u}(t) \rangle}{dt} \quad (4.4)$$

$$\frac{d\langle n_{C,u}(t) \rangle}{dt} = \check{K}_+ \ell(x_{R,u}, t) - k_- \langle n_{C,u}(t) \rangle \quad \text{for } u = 1, 2 \quad (4.5)$$

where $x_{T,a}$ (resp. $x_{R,u}$) is the centre of the voxel T_a (R_u) where the a -th transmitter (u -th receiver) is located. Note that we have also used the following conversion between the Kronecker and Dirac deltas: $\lim_{\Delta x \rightarrow 0} \frac{\delta_K(j)}{\Delta x} = \delta(x)$.

This shows that in the continuum, the RDMEX converges to a RDPDE (4.4) and a number of ODEs describing the kinetics at the receivers (4.5). The RDPDE (4.4) has a simple interpretation. The second term in (4.4) says that the transmitter at T_a adds signalling molecules to the system according to time sequence $k_a(t)$, while the third terms says the signalling molecules are absorbed from the system if they form complexes at the receivers. Given that we assume that one signalling molecule reacts to form one complex, therefore the rate of absorption of signalling molecules is equal to the rate of complex formation, which is given by (4.5).

Note that it is well known in the literature, see [14, 18], that a RDME with linear reaction rates converges to a RDPDE in continuum. In the above, we show analogous result holds for the RDMEX model.

Generalisation to 3-dimensional space

In order to simplify the presentation, we have so far limited to the 1-dimensional case. Given that most molecular communication networks are 3-dimensional, we state that in a 3-dimensional infinite medium the RDMEX will converge to the following RDPDE in the continuum. Here v

¹Note: We use both Kronecker delta and Dirac delta in this paper. They are denoted, respectively, as $\delta_K(\bullet)$ and $\delta(\bullet)$.

denotes a point in the 3-dimensional space (i.e. v is a 3-dimensional vector) and $\ell(v, t)$ is the mean concentration of the signalling molecule at the location v at time t .

$$\frac{\partial \ell}{\partial t} = D \nabla^2 \ell + \sum_{a=1}^2 \delta(v - v_{T,a}) k_a(t) - \sum_{u=1}^2 \delta(v - v_{R,u}) \frac{dc_u(t)}{dt} \quad (4.6)$$

$$\frac{dc_u(t)}{dt} = K_+ \ell(x_{R,u}, t) - k_- c_u(t) \text{ for } u = 1, 2 \quad (4.7)$$

where ∇^2 is the Laplacian in 3-dimensional space, and $v_{T,a}$ (resp. $v_{R,u}$) is a 3-dimensional vector specifying the location of a -th transmitter (u -th receiver). Note that we have also introduced a new notation $c_u(t)$ to denote the mean number of complexes $\langle n_{C,u}(t) \rangle$ at receiver u ; this is to simplify the notation later.

The derivation assumes that the molecule in a voxel diffuses to a neighbouring voxel at a rate of d per molecule per unit time and each voxel is a cube of size $(\Delta x)^3$. We require that in the limit, $d(\Delta x)^2 \rightarrow D$ and $k_+(\Delta x)^3 \rightarrow K_+$. Note that the latter condition is different from the 1-dimensional case. Given that the derivation for the 3-dimensional is essentially the same as the 1-dimensional case, we do not present it here.

4.2 Solution to RDPDE

In this section, we present a solution to the RDPDE (4.6) and (4.7), which is the continuum limit of 3-dimensional RDME model. The key result is a closed-form expression of the multivariate transfer function from the transmitter signals $k_1(t)$ and $k_2(t)$ (which models the number of molecules injected by the transmitter into the medium at time t and can be viewed as the inputs to the system) to the number of complexes formed at the receivers $c_1(t)$ and $c_2(t)$ (which can be viewed as the outputs). We will divide this section into two parts. We will first derive the transfer function and then provide an interpretation of the transfer function.

Derivation of transfer function

The aim of this part is to derive a multivariate transfer function from $k_1(t)$ and $k_2(t)$ to $c_1(t)$ and $c_2(t)$ using (4.6) and (4.7).

We first define a few notations. Let $\iota = \sqrt{-1}$, and $C_u(\omega)$, $K_a(\omega)$ and $\tilde{L}(v, \omega)$ be the temporal Fourier transform of, respectively, $c_u(t)$, $k_a(t)$ and $\ell(v, t)$ where ω is the transform variable. It is shown in Appendix A that

$$\tilde{L}(v, \omega) = \sum_{a=1}^2 \phi(v - v_{T,a}, \omega) K_a(\omega) - \sum_{u=1}^2 \phi(v - v_{R,u}, \omega) \iota \omega C_u(\omega) \quad (4.8)$$

where

$$\phi(v, \omega) = \frac{1}{4\pi D \|v\|} \exp\left(-\sqrt{\frac{\iota \omega}{D}} \|v\|\right) \quad (4.9)$$

is the temporal Fourier transform of the 3-dimensional diffusion kernel $\frac{1}{\sqrt{4\pi D t}} \exp(-\frac{\|v\|^2}{4Dt})$. Given (4.8) holds for any location v , we can use it to determine the concentration of the signalling molecules at the two receivers. By substituting $v = v_{R,1}$ and then $v = v_{R,2}$ in (4.8), we have:

$$\tilde{L}(v_{R,1}, \omega) = \phi_{11}(\omega) K_1(\omega) + \phi_{12}(\omega) K_2(\omega) - \phi_0(\omega) \iota \omega C_1(\omega) - \phi_{\Delta R}(\omega) \iota \omega C_2(\omega) \quad (4.10)$$

$$\tilde{L}(v_{R,2}, \omega) = \phi_{21}(\omega) K_1(\omega) + \phi_{22}(\omega) K_2(\omega) - \phi_{\Delta R}(\omega) \iota \omega C_1(\omega) - \phi_0(\omega) \iota \omega C_2(\omega) \quad (4.11)$$

where

$$\phi_{ua}(\omega) = \phi(v_{R,u} - v_{T,a}, \omega) \text{ for } u, a = 1, 2 \quad (4.12)$$

$$\phi_{\Delta R}(\omega) = \phi(v_{R,1} - v_{R,2}, \omega) \quad (4.13)$$

$$\phi_0(\omega) = \phi(\mathbf{0}, \omega) \text{ where } \mathbf{0} = \text{zero vector} \quad (4.14)$$

One can interpret $\phi_{ua}(\omega)$ as the transfer function which models the dynamics of the diffusion of molecules from the a -th transmitter located at $v_{T,a}$ (where the molecules are injected into the medium) to the u -th receiver located at $v_{R,u}$.

When signalling molecules are absorbed to form complexes, it creates a concentration gradient. The diffusion dynamics between the two receivers are modelled by $\phi_{\Delta R}(\omega)$. Given that we assume that the locations of the transmitters and receivers are distinct, both $\phi_{ua}(\omega)$ and $\phi_{\Delta R}(\omega)$ are well defined.

The transfer function $\phi_0(\omega)$ models the local impact of absorption of signalling molecule at each receiver. This transfer function is unfortunately not well defined as can be seen from substituting $v = \mathbf{0}$ in the definition of $\phi(v, \omega)$ in (4.9). The transfer function $\phi_0(\omega)$ also appears in the modelling of receptor noise in chemotaxis in the biophysics literature [6, 11]. In fact [6, Equation (18)] and [11, Equation (6)] are special cases of (4.6) where the input terms $k_a(t)$ are absent. Both [6, 11] deal with the indefiniteness of $\phi_0(\omega)$ by cutting off an integral to evaluate $\phi_0(\omega)$ at a finite frequency. However, this requires us to make an assumption on the size of the receptor molecule. Instead, in section 5, we derive a new method to approximate $\phi_0(\omega)$, and we will show using numerical examples in section 6 that our approximation gives accurate results. For the rest of this section, we will continue to use equations (4.10) and (4.11) with the understanding that $\phi_0(\omega)$ is not well defined but can be well approximated.

Both equations (4.10) and (4.11) are obtained from (4.6). We still need to work on (4.7). By taking the Fourier transform of (4.7), we have

$$\rho_1(\omega) = \frac{C_1(\omega)}{\tilde{L}(v_{R,1}, \omega)} = \frac{K_+}{\iota\omega + k_-} \quad (4.15)$$

$$\rho_2(\omega) = \frac{C_2(\omega)}{\tilde{L}(v_{R,2}, \omega)} = \frac{K_+}{\iota\omega + k_-} \quad (4.16)$$

where $\rho_1(\omega)$ and $\rho_2(\omega)$ are transfer functions that models the reaction dynamics at the receivers. Given that we have assumed that the binding and unbinding rate constants at both receivers are identical, it is not surprising that $\rho_1(\omega)$ and $\rho_2(\omega)$ are the same here. It is straightforward to generalise to the case where the receivers have different reaction dynamics.

By using equations (4.10), (4.11), (4.15) and (4.16), we can eliminate $\tilde{L}(v_{R,1}, \omega)$ and $\tilde{L}(v_{R,2}, \omega)$ to obtain the transfer function from the inputs $k_1(t)$ and $k_2(t)$ to the outputs $c_1(t)$ and $c_2(t)$:

$$\begin{bmatrix} C_1 \\ C_2 \end{bmatrix} = \left(I + \iota\omega \underbrace{\begin{bmatrix} \rho_1 & 0 \\ 0 & \rho_2 \end{bmatrix}}_{\mathcal{R}} \underbrace{\begin{bmatrix} \phi_0 & \phi_{\Delta r} \\ \phi_{\Delta r} & \phi_0 \end{bmatrix}}_{\Phi_0} \right)^{-1} \begin{bmatrix} \rho_1 & 0 \\ 0 & \rho_2 \end{bmatrix} \underbrace{\begin{bmatrix} \phi_{11} & \phi_{12} \\ \phi_{21} & \phi_{22} \end{bmatrix}}_{\Phi} \begin{bmatrix} K_1 \\ K_2 \end{bmatrix} \quad (4.17)$$

where, for conciseness, we have dropped the dependence on transform variable ω . Equation (4.17) is the key result of this section. It is the solution to the RDPDE (4.6) and (4.7), which are in turn the continuum limit of the mean concentration in the stochastic RDMEX model. We will provide some physical interpretation of (4.17) in a moment. Before that, we want to point out that (4.17) can be used to compute $c_1(t)$ and $c_2(t)$ given $k_1(t)$, $k_2(t)$ and the system parameters by numerical Laplace transform. This will be done in Section 6.

Interpretation of transfer function (4.17)

Equation (4.17) may not look easy to interpret in the first instance, so we will first specialise it to the case of 1-transmitter and 1-receiver. In this case, we have

$$C_1 = \frac{\rho_1 \phi_{11}}{1 + \iota\omega \phi_0 \rho_1} K_1 \quad (4.18)$$

One can readily show that the input-output transfer function in (4.18) corresponds to the block diagram representation of figure 4.1. The negative feedback loop occurs because the net

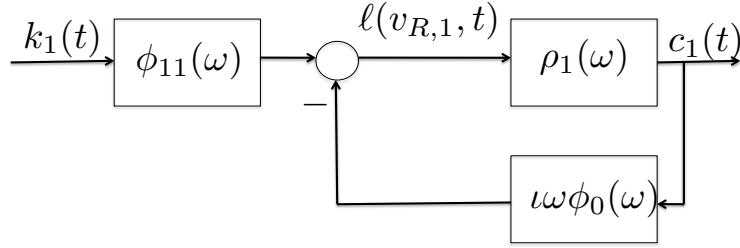


Figure 4.1: Block diagram showing the transfer function from the input $k_1(t)$ to the output $c_1(t)$ of a molecular communication network with one transmitter and one receiver.

number of signalling molecules at the receiver $\ell(v_{R,1}, t)$ is given by the difference between those that arrive via diffusion (modelled by the feedforward block of ϕ_{11}) minus those reacted to form the complexes (modelled by the feedback block of $i\omega\phi_0$). The forward loop consists of ϕ_{11} which models the diffusion dynamics of signalling molecule from the location of the transmitter to that of the receiver, and ρ_1 which models the conversion of the signalling molecules to complexes.

We will now take a closer look at the denominator of (4.18) with the aim to determine the strength of the feedback term $i\omega\phi_0\rho_1$. It has been shown in [6, 11] that $\phi_0 \propto \frac{1}{2\pi D}$ at low frequency. Consider the case where $D \gg K_+$ or $\frac{K_+}{D} \approx 0$, which corresponds to the situation where the chemical kinetics is not diffusion-limited. We have $i\omega\phi_0\rho_1 \approx 0$ based on the expression of ρ_1 in (4.15) and consequently $C_1 = \rho_1\phi_{11}K_1$. Since the chemical kinetics is not diffusion-limited, the chemical kinetics and diffusion are basically "decoupled", so the transfer function from K_1 to C_1 is the multiplication of the transfer function ϕ_{11} from k_1 to $\ell(v_{R,1}, t)$ (which models diffusion) and the transfer function ρ_1 from $\ell(v_{R,1}, t)$ to c_1 (which models kinetics). We will show in section 6 using numerical examples to show that the transfer function $\frac{\rho_1\phi_{11}}{1+i\omega\phi_0\rho_1} \approx \rho_1\phi_{11}$ holds when $D \gg K_+$.

An end-to-end frequency model for molecular communication with one transmitter and one receiver has earlier been derived in [24]. The model assumes decoupling of diffusion and chemical kinetics [24, Equation 1] which means that the model in [24] corresponds to the case where chemical kinetics is not diffusion-limited.

Given the interpretation of the 1-transmitter 1-receiver case as a system with feedback in figure 4.1, it can be shown that equation (4.17) corresponds to multivariate feedback system with 2 inputs and 2 outputs. The block structure of the multivariate feedback system is the same as that in figure 4.1 but we need to replace the single-input single-output transfer functions ϕ_{11} , ρ_1 and ϕ_0 by their multivariate counterparts of Φ_1 , \mathcal{R} and Φ_0 in (4.17).

For the 2-transmitter 2-receiver case, we see from (4.17) that the response at each receiver is affected by both transmitters, as well as by the other receiver. Let us assume that the transmitters and receivers form two communication pairs where transmitters 1 and 2 intend to communicate with, respectively, receivers 1 and 2. We want to determine the amount of interference at the receivers. Let us assume for the time being that the two receivers are sufficiently far apart so that $\phi_{\Delta r}(\omega)$ is negligible compared with $\phi_0(\omega)$. In addition, we assume the two receivers are identical, so $\rho_1(\omega) = \rho_2(\omega)$. In this case, we can simplify (4.17) to

$$\begin{bmatrix} C_1 \\ C_2 \end{bmatrix} = \frac{\rho_1}{1 + i\omega\phi_0\rho_1} \begin{bmatrix} \phi_{11} & \phi_{12} \\ \phi_{21} & \phi_{22} \end{bmatrix} \begin{bmatrix} K_1 \\ K_2 \end{bmatrix} \quad (4.19)$$

Comparing with the single-transmitter single-receiver transfer function in (4.17), we can see that the interference of transmitter 2 on receiver 1 is $\frac{\rho_1\phi_{12}}{1+i\omega\phi_0\rho_1}K_2$. One can readily see that this interference can be reduced if transmitter 2 is well separated in space from receiver 1 because ϕ is a decreasing function of distance. Similar conclusion can be drawn for transmitter 1 and receiver 2. Note that the above argument requires that the receivers are well separated. If this is not the case, the matrix inverse in (4.17) will create a complicated mixture of signal at both receivers.

In general, spatial separation is a strategy to reduce the amount of interference that one communication pair has on the others. It is interesting to point out that (4.17) allows one to explore other methods to reduce this interference. An interesting case to study is if the transmitters emit molecules at different frequencies and the receivers are frequency sensitive. We will not explore this further here and leave this for future work.

5 Discrete solution for mean concentration in RDMEX

In the last section, we presented a closed-form solution to the RDPDE (4.6). A problem that we face is that the frequency response $\phi_0(\omega)$ in (4.14) is not well defined. This problem arises because the size of voxel, in the continuum limit, becomes zero. Therefore, a solution to overcome this problem is to consider finite voxel size instead. This means that we need to work with the 3-dimensional analogue of equations (4.2) and (4.3).

Consider an isotropic 3-dimensional space. We divide the space into identical cubic voxels of volume Δ^3 each. We index the voxel using a 3-dimensional vector $\xi = [i \ j \ k]$ where $i, j, k \in \mathbb{Z}$; note that we will use ξ and $[i \ j \ k]$ interchangeably in this section. We use $\xi_{T,a}$ ($\xi_{R,u}$) to index the voxel that the a -th transmitter (u -th receiver) is located. We will also use $\ell_{R,u}$ to denote the mean concentration of signalling molecules at the voxel where the u -th receiver is located. Let $\tilde{c}_u(t)$ denote the mean number of complexes at the u -th receiver for this discrete model and $\tilde{C}_u(\omega)$ be its continuous Fourier transform. (Just to avoid any possible confusion. We discretise only space, not time. So, t remains continuous.)

Let $\ell_{i,j,k}(t)$ denotes the mean concentration of the signalling molecule in voxel i, j, k . The mean concentration in a voxel is given by the mean number of molecules divided by the volume of a voxel which is Δ^3 . One can show that the generalisation of (4.2) and (4.3) to 3-dimensional space — with mean concentration of signalling molecules, rather than mean number, per voxel — is:

$$\begin{aligned} \frac{d\ell_{i,j,k}(t)}{dt} &= \tilde{D}(\ell_{i-1,j,k}(t) - 2\ell_{i,j,k}(t) + \ell_{i+1,j,k}(t)) + \\ &\quad \tilde{D}(\ell_{i,j-1,k}(t) - 2\ell_{i,j,k}(t) + \ell_{i,j+1,k}(t)) + \\ &\quad \tilde{D}(\ell_{i,j,k-1}(t) - 2\ell_{i,j,k}(t) + \ell_{i,j,k+1}(t)) + \\ &\quad \sum_{a=1}^2 \frac{1}{\Delta^3} \delta_K(\xi - \xi_{T,a}) k_a(t) - \sum_{u=1}^2 \frac{1}{\Delta^3} \delta_K(\xi - \xi_{R,u}) \frac{d\tilde{c}_u(t)}{dt} \end{aligned} \quad (5.1)$$

$$\frac{d\tilde{c}_u(t)}{dt} = \tilde{K}_+ \ell_{R,u} - k_- \tilde{c}_u(t) \text{ for } u = 1, 2 \quad (5.2)$$

where $\tilde{D} = \frac{\mathcal{D}}{\Delta^2}$, $\tilde{K}_+ = k_- \Delta^3$. One can readily show that the continuum limit of (5.1) and (5.2) is (4.6) and (4.7)

Let $\tilde{L}_d(\xi, \omega)$ denote the temporal Fourier transform of $\ell_{i,j,k}(t)$. By using multi-dimensional z -transform, it is shown in Appendix B that

$$\tilde{L}_d(\xi, \omega) = \sum_{a=1}^2 \psi(\xi - \xi_{T,a}, \omega) K_a(\omega) - \sum_{u=1}^2 \psi(\xi - \xi_{R,u}, \omega) \iota \omega \tilde{C}_u(\omega) \quad (5.3)$$

where

$$\psi(v = [i, j, k], \omega) = \frac{1}{4\pi^2 \tilde{D} \Delta} \oint_{\mathcal{C}} \oint_{\mathcal{C}} \frac{W_{z^*}^{|k|+1}}{W_{z^*}^2 - 1} W_x^{i-1} W_y^{j-1} dW_x dW_y \quad (5.4)$$

where W_x and W_y are complex variables and the contour \mathcal{C} is the unit circle on the complex plane; also, W_{z^*} is the solution of the following quadratic equation in W_z with modulus less than unity:

$$W_z^2 - (2 + (W_x - W_x^{-1})^2 + (W_y - W_y^{-1})^2 + \iota \omega \frac{\Delta^2}{\tilde{D}}) W_z + 1 = 0 \quad (5.5)$$

Note that (5.3) is the discrete space analogue of (4.8). Thus one can identify $\phi(\mathbf{0}, \omega)$ with $\psi(\mathbf{0}, \omega)$. In addition, one can show that:

$$\begin{bmatrix} \bar{C}_1 \\ \bar{C}_2 \end{bmatrix} = \left(I + \iota\omega \begin{bmatrix} \rho_1 & 0 \\ 0 & \rho_2 \end{bmatrix} \begin{bmatrix} \psi_0 & \psi_{\Delta r} \\ \psi_{\Delta r} & \psi_0 \end{bmatrix} \right)^{-1} \begin{bmatrix} \rho_1 & 0 \\ 0 & \rho_2 \end{bmatrix} \begin{bmatrix} \psi_{11} & \psi_{12} \\ \psi_{21} & \psi_{22} \end{bmatrix} \begin{bmatrix} K_1 \\ K_2 \end{bmatrix} \quad (5.6)$$

where for conciseness we have dropped the dependence on ω , and $\psi_{ua}(\omega) = \psi(\xi_{R,u} - \xi_{T,a}, \omega)$, $\psi_{\Delta r}(\omega) = \psi(\xi_{R,1} - \xi_{R,2}, \omega)$ and $\psi_0(\omega) = \psi(\mathbf{0}, \omega)$.

Numerical integration can be used to compute $\psi(\xi, \omega)$ in (5.4). This will be used in Section 6.

6 Numerical examples

In this section, we will give a number of numerical examples to show that the solutions to (4.8) in section 4.2 and (5.3) in section 5 can be used to accurately predict the mean output of the receivers in the stochastic model RDMEX.

We will use simulation to determine the mean behaviour of RDMEX. One method is to simulate RDMEX many times and compute the mean. Alternatively, one can use the fact that if the number of molecules is large, then the behaviour of one simulation run is fairly close to the mean. We will use the latter method in this paper. We simulate the RDMEX model using the τ -leaping method [15]. The τ -leaping algorithm uses a constant time step to advance the simulation and is a faster alternative to the Gillespie's algorithm [15]. We will refer to the simulation result as RDMEX- τ .

We will present two sets of results: single-transmitter single-receiver in section 6.1 and two-transmitter two-receiver in 6.2. The fluidic medium is assumed to have a D of 0.05. (Since the parameters in the diffusion-reaction system can be scaled to some dimensionless quantities [9, Section 8.2], we do not specify the units for the parameters here.) The locations of the transmitters and receivers, as well as the reaction rate constants, vary between experiments and will be specified later. In all the experiments, the transmitters emit 10 molecules every 10^{-4} time units for a duration of 0.2 time units and then stops emitting for 0.3 time units. The signals $k_1(t)$ and $k_2(t)$ are obtained by concatenating this emission pattern 3 times. The simulation time is 2 time units. Our goal is to compare the output $c_1(t)$ and $c_2(t)$ from RDMEX- τ with that from the following analytical models:

1. Equation (4.8) of the continuum model with $\phi(\mathbf{0}, \omega)$ replaced by $\psi(\mathbf{0}, \omega)$. We will refer to this as RDPDE.
2. Equation (5.3). We will refer to this as RDMEX-M.
3. Equation (4.8) of the continuum model with $\phi(\mathbf{0}, \omega)$ approximated by $\frac{1}{2\pi D \Delta}$. This approximation is inspired by the one used in [6, 11] where we have replaced the size of receptors by the voxel dimension parameter Δ . We will refer to this as RDPDE-X.
4. For the single-transmitter and single-receiver case, we consider the ‘‘decoupled’’ model $C_1 = \rho_1 \phi_{11} K_1$. This will be referred to as DE.

For all these analytical models, we first determine the Laplace transforms C_1 and C_2 by using the Laplace transforms K_1 and K_2 , and the transfer function. We then perform inverse Laplace transform numerically using matlab [17].

6.1 Single-transmitter single-receiver case

The system consists of a transmitter at the voxel $[0, 0, 0]$ and a receiver at voxel $[3, 0, 0]$. Two different values of K will be used. Figure 6.1 shows the results for $K = 2.5 \times 10^{-3}$. The figure compares the mean number of complexes formed in the time interval $[0, 2]$. Results are obtained from RDMEX- τ (simulation) and RDPDE, RDMEX-M, RDPDE-X and DE (analytical models).

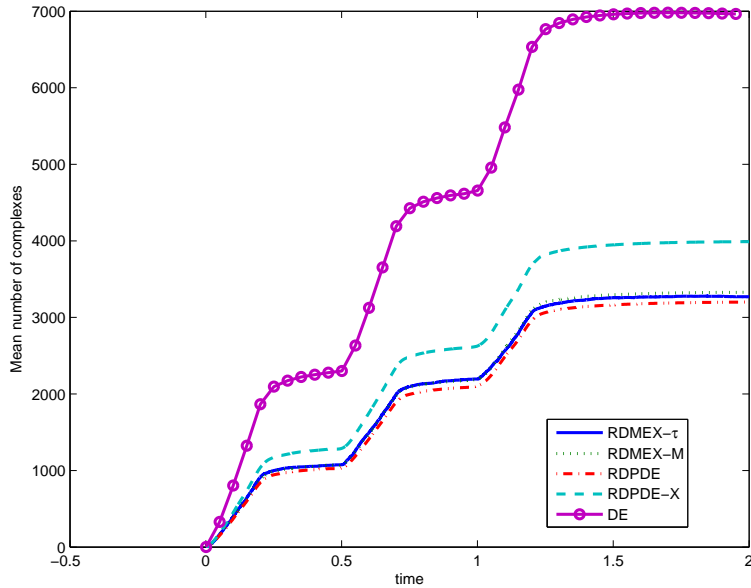


Figure 6.1: The mean number of complexes in the 1-transmitter 1-receiver network for $K = 2.5 \times 10^{-3}$.

It can be seen that both RDPDE and RDMEX-M match RDMEX- τ well. The model RDPDE-X does not give good approximation because the voxel size is not a good approximation for the receptor size. Henceforth, we will not consider RDPDE-X further. The decoupled model DE does not match RDMEX- τ for this value of K .

We keep the transmitter and receiver at the same location, and change K to 2.5×10^{-4} . Both RDMEX-M and RDPDE again match RDMEX- τ well. We also see that the decoupled model DE gives better prediction than before. This validates the discussion in Section 4.2 that the decoupled model holds when K is sufficiently small.

6.2 Two-transmitter Two-receiver case

We consider a molecular communication network with 2 transmitters (located at $[0, 0, 0]$ and $[4, 0, 0]$) and 2 receivers (located at $[1, 1, 0]$ and $[2, 0, 1]$). Both transmitters use the same emission pattern mentioned in the beginning of the section. We are interested in the mean number of complexes formed at the two receivers. Figures 6.3 and 6.4 show the results for, respectively, receivers 1 and 2. The three curves in each figure are obtained from RDMEX- τ (simulation) and RDPDE and RDMEX-M (analytical models). It can be seen from both figures that the prediction from both RDPDE and RDMEX-M match that of RDMEX- τ .

7 Related work

Molecular communication networks can be divided into two categories, according to whether it is natural or synthetic. Natural molecular communication networks are prevalent in living organisms. Their synthetic counterparts, though still rare, do exist. For example, [5] presents a system with multiple genetically engineered cells that use cell signalling to coordinate their behaviour.

The modelling of natural and synthetic molecular communication networks is studied in different disciplines. The former is mainly studied in biophysics and mathematical physiology, while the latter in synthetic biology. There is also a recent interest in the engineering community to

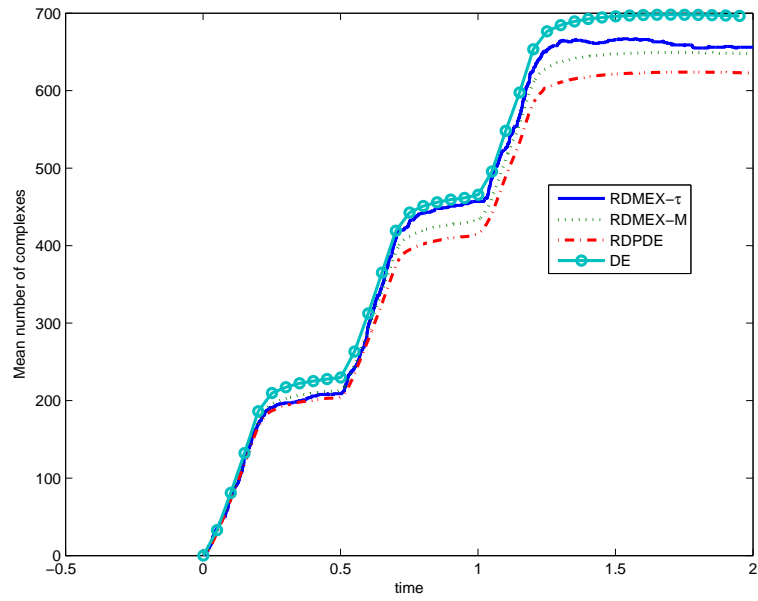


Figure 6.2: The mean number of complexes in the 1-transmitter 1-receiver network for $K = 2.5 \times 10^{-4}$.

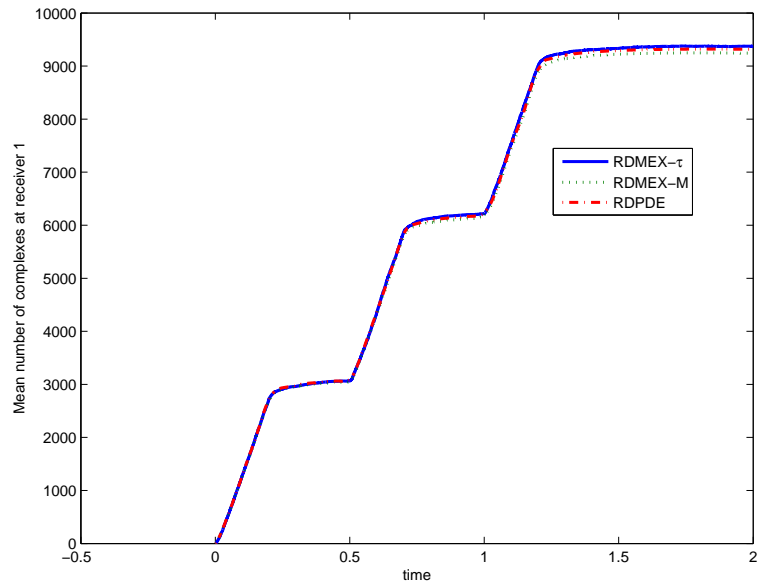


Figure 6.3: The mean number of complexes at receiver 1 in the 2-transmitter 2-receiver network.

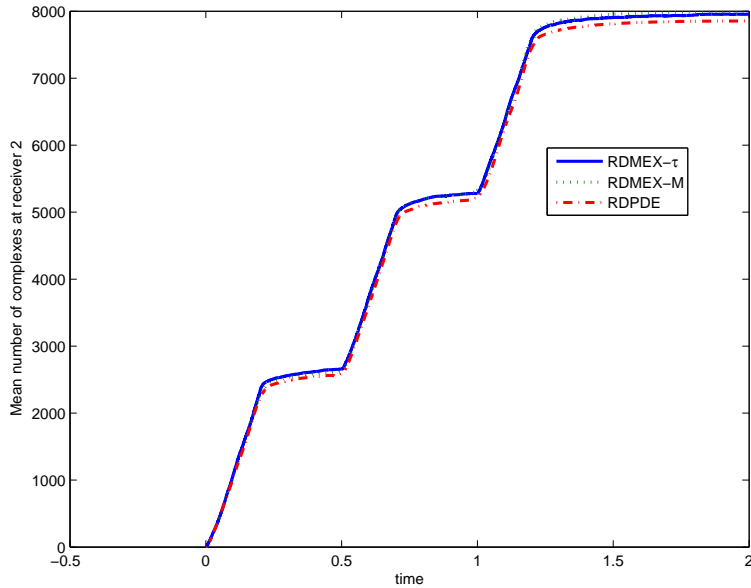


Figure 6.4: The mean number of complexes at receiver 2 in the 2-transmitter 2-receiver network.

study molecular communication networks from a communication theory point of view. This gives rise to a new research area called nano communication networks [1].

Despite the fact that molecular communication networks are studied in diverse disciplines, the set of mathematical models that are being used are similar. This is not surprising given that the primary goal is to model diffusion and reaction kinetics. The classes of mathematical models being used include molecular dynamics, master equation, partial differential equation (PDE), Fokker-Planck equation, Langevin equation and so on. We will focus on the first three classes of models in this discussion.

Molecular dynamics is commonly used in simulation of molecular communication networks. Many examples of simulators exist, especially for natural molecular communication networks, see [7] for a recent overview. For synthetic networks, a recent example is [16]. By analysing the molecular dynamics of transmitters and receivers, [25] characterises the noise in transmitters and receivers as, respectively, sampling and counting noise.

There are plenty of examples in using PDE, in particular diffusion PDE, telegraph equation and RDPDE, to model molecular communications. For natural networks, [6, 11] use RDPDE to study the noise in receptor binding in chemotaxis, and [23] uses RDPDE to study signalling cascades. For synthetic networks, telegraph or diffusion PDEs (or their kernels) have been used to characterise the diffusion of signalling molecules in [26, 22, 2, 4] and others. In our earlier work in [8], we use a RDPDE in the form of (4.6), as a deterministic model for molecular communication network. The RDPDE in [8] is solved numerically and no analytic solution is provided.

For some time, RDME has been considered to be a phenomenological model because it diverges in certain cases [19]. Fortunately, the problem has been resolved in [13] and there is now a firm theoretic basis for RDME. Examples of work that use RDME to model natural molecular communication networks include [18, 10]. To the best of our knowledge, our method of coupling a deterministic (or mean) molecule emission pattern with RDME to model molecular communication networks has not been considered before. The proposed RDMEX model is one of the novel contributions of this paper to the modelling of molecular communication networks.

8 Conclusions

In this paper, we have proposed a new stochastic model called reaction-diffusion master equation with exogenous input (RDMEX) for modelling molecular communication networks with multiple transmitters and multiple receivers. We show that we can readily derive the mean and covariance behaviour of RDMEX model. We then solve the mean behaviour of RDMEX model using two different methods. In the first method, we derive the continuum limit of RDMEX and present a close-form expression of the solution to the resulting reaction-diffusion partial differential equation. In the second method, we solve the mean behaviour of RDMEX explicitly by using transform techniques. We present numerical examples comparing the accuracy of our analytical solutions against simulation. We find our analytical solutions fairly accurate.

Appendix

A Derivation of (4.8)

Equation (4.8) can be derived by using a couple of different methods, e.g. Fourier transform or Green's function. We will use Green's function here.

Note that the RDPDE (4.6) is an inhomogeneous partial differential equation where the last two terms act as the forcing function. Let $G(v, t)$ denote the three dimensional kernel of the linear diffusion equation $\frac{\partial \ell}{\partial t} = D \nabla^2 \ell$. Let also $*_{S,T}$ denote convolution in space and time, and $*_T$ denote convolution in time only. By using the theory of Green's function, we have

$$\begin{aligned} \ell(v, t) &= G(v, t) *_{S,T} \left\{ \sum_{a=1}^2 \delta(v - v_{T,a}) k_a(t) - \sum_{u=1}^2 \delta(v - v_{R,u}) \frac{dc_u(t)}{dt} \right\} \\ &= \sum_{a=1}^2 G(v - v_{T,a}, t) *_T k_a(t) - \sum_{u=1}^2 G(v - v_{R,u}, t) *_T \frac{dc_u(t)}{dt} \end{aligned} \quad (\text{A.1})$$

Now we can obtain (4.8) from applying temporal Fourier transform to (A.1), noting that $\phi(v, \omega)$ is the temporal Fourier transform of $G(v, t)$.

B Derivation of (5.3)

Note that (5.1) is a linear difference equation in space and a continuous differential equation in time. We can draw a parallel with the theory of Green's function and note that (5.3) holds if $\psi(\xi, \omega)$ is the temporal Fourier transform of the solution of the following equation:

$$\begin{aligned} \frac{dh_{i,j,k}(t)}{dt} &= \tilde{D}(h_{i-1,j,k}(t) - 2h_{i,j,k}(t) + h_{i+1,j,k}(t)) + \tilde{D}(h_{i,j-1,k}(t) - 2h_{i,j,k}(t) + h_{i,j+1,k}(t)) + \\ &\quad \tilde{D}(h_{i,j,k-1}(t) - 2h_{i,j,k}(t) + h_{i,j,k+1}(t)) + \frac{1}{\Delta^3} \delta_K(\xi) \delta(t) \end{aligned} \quad (\text{B.1})$$

This equation can be solved by using Fourier transform on the continuous variable t and z-transform on the discrete variables i, j and k . Let $H_{i,j,k}(\omega)$ denote the Fourier transform of $h_{i,j,k}(t)$. The multi-dimensional z-transform of $H_{i,j,k}(\omega)$ is defined as:

$$\Psi(W_x, W_y, W_z, \omega) = \sum_{i=-\infty}^{\infty} \sum_{j=-\infty}^{\infty} \sum_{k=-\infty}^{\infty} H_{i,j,k}(\omega) W_x^{-i} W_y^{-j} W_z^{-k} \quad (\text{B.2})$$

By using (B.1), it can be shown that

$$\Psi(W_x, W_y, W_z, \omega) = \frac{-1}{\tilde{D} \Delta \{ (W_x - W_x^{-1})^2 + (W_y - W_y^{-1})^2 + (W_z - W_z^{-1})^2 - \frac{i\omega \Delta^2}{D} \}} \quad (\text{B.3})$$

We first compute inverse z-transform with respect to W_z and write (B.3) as

$$\Psi(W_x, W_y, W_z, \omega) = \frac{-1}{\tilde{D}\Delta} \frac{W_z}{(W_z - W_{z*})(W_z - W_{z*}^{-1})} \quad (\text{B.4})$$

where W_{z*} , as defined in section 5, is root of (5.5) with modulus less than unity. Note we have also used the fact the roots of (5.5) are reciprocal of each other. It can now be shown that the inverse z-transform of $\Psi(W_x, W_y, W_z, \omega)$ with respect to W_z is

$$\frac{-1}{\tilde{D}\Delta} \frac{W_{z*}^{|k|+1}}{W_{z*}^2 - 1} \quad (\text{B.5})$$

If we apply the standard inverse z-transform contour integrals, with respect to W_x and W_y , to this expression, then we obtain the formula for $\psi(v, \omega)$ given in (5.4).

Bibliography

- [1] I Akyildiz, F Brunetti, and C Blázquez. Nanonetworks: A new communication paradigm. *Computer Networks*, 52:2260–2279, 2008.
- [2] D Arifler. Capacity analysis of a diffusion-based short-range molecular nano-communication channel. *Computer Networks*, 55:1426–1434, 2010.
- [3] B Atakan, O.B Akan, and S Balasubramaniam. Body area nanonetworks with molecular communications in nanomedicine. *Communications Magazine, IEEE*, 50(1):28–34, 2012.
- [4] Baris Atakan and Ozgur B Akan. Deterministic capacity of information flow in molecular nanonetworks. *Nano Communication Networks*, 1(1):31–42, May 2010.
- [5] Subhayu Basu, Yoram Gerchman, Cynthia H Collins, Frances H Arnold, and Ron Weiss. A synthetic multicellular system for programmed pattern formation. *Nature*, 434(7037):1130–1134, April 2005.
- [6] W Bialek and S. Setayeshgar. Physical limits to biochemical signaling. *Proceedings of the National Academy of Sciences*, 102(29):10040–10045, 2005.
- [7] K Burrage, PM Burrage, A Leier, T Marquez-Lago, and DV Nicolau Jr. Stochastic simulation for spatial modelling of dynamic processes in a living cell. *Design and Analysis of Bio-molecular Circuits*, page 43, 2011.
- [8] C.T. Chou. Molecular circuits for decoding frequency coded signals in nano-communication networks. *Nano Communication Networks*, 2012. <http://www.sciencedirect.com/science/article/pii/S1878778911000676>.
- [9] J. Crank. *The mathematics of diffusion*. OUP, 1980.
- [10] J Elf. Spontaneous separation of bi-stable biochemical systems into spatial domains of opposite phases. *Systems Biology*, 1(2):230–236, 2004.
- [11] RG Endres and NS Wingreen. Accuracy of direct gradient sensing by cell-surface receptors. *Progress in biophysics and molecular biology*, 100(1-3):33–39, 2009.
- [12] Radek Erban, Jonathan Chapman, and Philip Maini. A practical guide to stochastic simulations of reaction-diffusion processes. *arXiv, q-bio.SC*, April 2007.
- [13] D Fange, O Berg, P Sjöberg, and J Elf. Stochastic reaction-diffusion kinetics in the microscopic limit. *Proceedings of the National Academy of Sciences*, 107(46):19820–19825, 2010.
- [14] C. Gardiner. *Stochastic methods*. Springer, 2010.

- [15] D Gillespie. Stochastic simulation of chemical kinetics. *Annual review of physical chemistry*, 2007.
- [16] Ertan Gul, Baris Atakan, and Ozgur B Akan. NanoNS: A nanoscale network simulator framework for molecular communications. *Nano Communication Networks*, 1(2):138–156, September 2010.
- [17] K. J. Hollenbeck. *INVLAP.M: A matlab function for numerical inversion of Laplace transforms by the de Hoog algorithm*, 1998. <http://www.isva.dtu.dk/staff/karl/invlap.htm>.
- [18] SA Isaacson and CS Peskin. Incorporating diffusion in complex geometries into stochastic chemical kinetics simulations. *SIAM Journal on Scientific Computing*, 28(1):47–74, 2007.
- [19] Samuel Isaacson. Relationship between the reaction–diffusion master equation and particle tracking models. *Journal of Physics A: Mathematical and Theoretical*, 41:065003, February 2008.
- [20] I Lestas, J Paulsson, N Ross, and G Vinnicombe. Noise in gene regulatory networks. *IEEE Transactions on Automatic Control*, 53(1):198–200, 2008.
- [21] L. Ljung. *System identification - Theory for the user*. Prentice Hall, 2nd edition, 1999.
- [22] M Mahfuz, D Makrakis, and Hussein Mouftah. On the characterization of binary concentration-encoded molecular communication in nanonetworks. *Nano Communication Networks*, 1:289–300, 2010.
- [23] Z Neufeld and B Kholodenko. Positional information generated by spatially distributed signaling cascades. *PLoS Computational Biology*, 5(3), 2009.
- [24] M Pierobon and Ian F Akyildiz. A physical end-to-end model for molecular communication in nanonetworks. *IEEE JOURNAL ON SELECTED AREAS IN COMMUNICATIONS*, 28(4):602–611, 2010.
- [25] M Pierobon and Ian F Akyildiz. Diffusion-based Noise Analysis for Molecular Communication in Nanonetworks. *IEEE TRANSACTIONS ON SIGNAL PROCESSING*, 59(6):2532–2547, 2011.
- [26] M Pierobon and Ian F Akyildiz. Noise Analysis in Ligand-Binding Reception for Molecular Communication in Nanonetworks. *IEEE TRANSACTIONS ON SIGNAL PROCESSING*, 59(9):4168–4182, 2011.
- [27] N.G. van Kampen, editor. *Stochastic Processes in Physics and Chemistry*. North-Holland, 3rd edition, 2007.
- [28] Z Xie, L Wroblewska, L Prochazka, R Weiss, and Y Benenson. Multi-Input RNAi-Based Logic Circuit for Identification of Specific Cancer Cells. *Science*, 333(6047):1307–1311, September 2011.